

Analysis of Ultrasonic Pulse Generated by Piezoelectric Material (LiNbO3 Cut Y-X) Using SVM Classifier

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Abstract— In this paper, we propose a new numerical method for ultrasonic pulse detection of an acoustics microwaves signal during the propagation of acoustics microwaves generated by piezoelectric substrate LiNbO3 Cut Y-X in ultrasonic transducer. We have used the classifications by support vector machines (SVM) , the originality of this method is it provides the accurate values and help us to identify undetectable waves that we can not identify with the classical methods; in which we classify all the values of the real part and the imaginary part of the coefficient attenuation with the acoustic velocity in order to build a model from which we note the Ultrasonic Pulse or microwaves acoustics (bulk waves). By which we obtain accurate values for each of the coefficient attenuation and acoustic velocity. This study will be very interesting in modeling and realization of acoustics microwaves devices (ultrasound) based on the propagation of acoustics microwaves.

Keywords— Ultrasonic ; Piezoelectric material ; Support Vector Machines (SVM); Classification

I. INTRODUCTION

Medical diagnostic ultrasound is an imaging modality that makes images showing a slice of the body, so-called tomographic images (tomo = Gr. tome, to cut and graphic = Gr. graphein, to write). It is a diagnostic modality, meaning that it gathers information about the biological medium without modification of any kind (Figure 1) the ultrasonic transducer is the one responsible for generating ultrasound and recording the echoes generated by the medium. Since the transducer should make mechanical vibrations in the megahertz range, a material that can vibrate that fast is needed. Piezoelectric materials are ideal for this. (Figure 2)

The interest in the use of piezoelectric materials as the wave propagation medium, lies in the propagation of

appearance. These waves, in this case, spread in a resilient part (or Ultrasonic Pulse) and power; hence the name electro elastic or electroacoustic [1]. This coupling allows the piezoelectric waves that propagate acoustic velocities to be very stable with frequencies. The resulting material will be considered a delay structure and allows an efficient signal processing [2].

So the processed signal is applied to the electrodes of the transducer which in turn leads to deformation (compression and expansion) and a piezoelectric wave arises is propagating in the X direction (Figure 2) [2][3][4].

In our case, we propose another approach for the modelling of the acoustic microwaves with a complementary vision to the literature mentioned above. In this approach we interested especially in the detection of ultrasonics by the use of a (SVM) as detection tool in order to mark the mode of a ultrasonics.

In this work, we searched for all Acoustic velocity and Attenuation coefficients relying on fundamental relations and we classified all the values so that we can detect Ultrasonic Pulse easily.

II. PHENOMENOLOGICAL TENSORIAL PIEZOELECTRIC EQUATIONS

The signal to be treated will be applied to the electrodes of the transducer that generates the distortions (compression and dilatation), so a piezoelectric wave is generated and propagated in the X direction . We consider the space coordinates as follows:

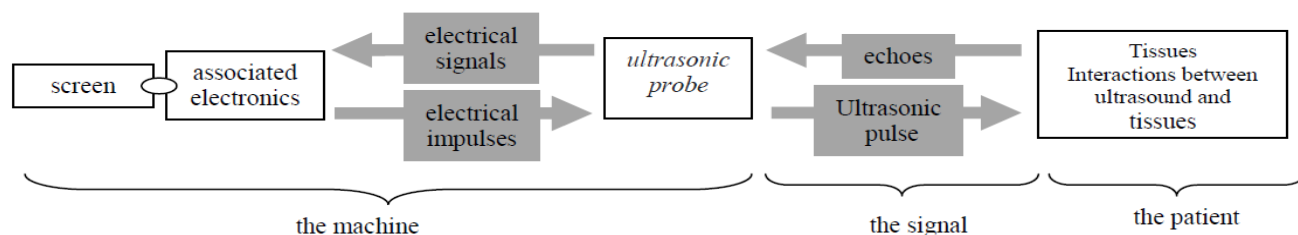


Figure 1 . principle of ultrasound diagnosis

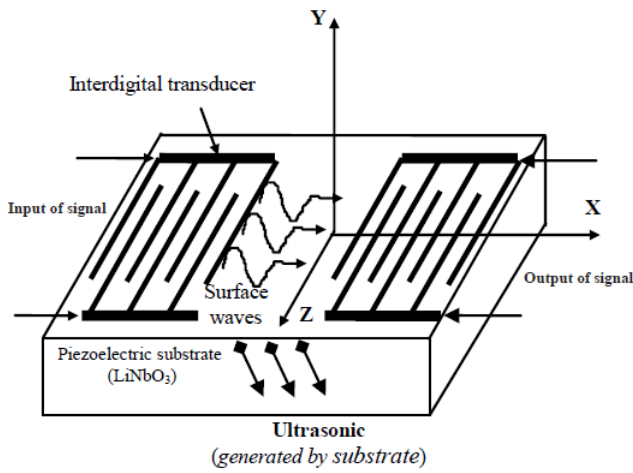


Figure 2. Ultrasonic Pulse generated by LiNbO3 substrate

$$X=X_1, Y=X_2, Z=X_3$$

The mechanical state of the medium is defined by two magnitudes of tensorial type, the stress T_{ij} and the mechanical deformation (Strain) S_{ij} ($i, j=1, 2, 3$).

The electric state of the medium is defined by two vectors, the electric field E_k and the electric induction D_i . The stress tensor and the electric induction are defined like follows [5]:

$$T_{ij} = C_{ijkl} S_{kl} - e_{kij} E_k \quad (1)$$

$$D_i = e_{jkl} S_{kl} + \varepsilon_{ik} E_k \quad (2)$$

with $i, j, k, l=1, 2, 3$, where

- ε_{ik} : permittivity tensor (F/m)
- e_{jkl} : piezoelectric tensor (c/m)
- C_{ijkl} : elastic tensor (N/m²)

The strain is bound to the relative displacements of the particles of the material environment is defined by :

$$S_{ij} = \frac{1}{2} \left(\frac{\partial u_i}{\partial X_j} + \frac{\partial u_j}{\partial X_i} \right) \quad (3)$$

where U_i represents the elastic displacement of the particle ($i=1, 2, 3$).

Note that, in the quasi-static approximation, an electric field of component can be defined by [6,7]:

$$E_i = -\frac{\partial U_4}{\partial X_i} \quad (4)$$

where U_4 is the electric potential (with $i=1, 2, 3$)

On the other hand, in the quasi-static approximation, the Maxwell's equation amounts to the Poisson's equation [5-7].

$$\text{div} \vec{D} = \frac{\partial D_i}{\partial X_i} = 0 \quad (5)$$

The movement of the particles under the action of stress (constraints), is described by the following differential equation (Newton's 2nd law) [8-9]

$$\nabla T = \rho \frac{\partial^2 U_j}{\partial t^2} \quad (6)$$

where ρ is the mass density of medium.

Replacing (3) and (4) in (1) and (2), we obtain

$$T_{ij} = C_{ijkl} \cdot \frac{1}{2} \left(\frac{\partial u_j}{\partial X_k} + \frac{\partial u_k}{\partial X_j} \right) + e_{kij} \cdot \frac{\partial U_4}{\partial X_k} \quad (7)$$

$$D_{ij} = e_{ikl} \cdot \frac{1}{2} \left(\frac{\partial u_j}{\partial X_k} + \frac{\partial u_k}{\partial X_j} \right) - \varepsilon_{ik} \cdot \frac{\partial U_4}{\partial X_k} \quad (8)$$

Replacing (7) and (8) in (5) and (6), we obtain

$$C_{ijkl} \frac{\partial^2 u_k}{\partial X_i \partial X_l} + e_{lij} \frac{\partial^2 U_4}{\partial X_k \partial X_i} = \rho \frac{\partial^2 U_j}{\partial t^2} \quad (9)$$

$$e_{ikl} \frac{\partial^2 U_k}{\partial X_i \partial X_l} - \varepsilon_{ik} \frac{\partial^2 U_4}{\partial X_k \partial X_i} = 0 \quad (10)$$

Equations (9) and (10) are the piezoelectric tensorial equations, they characterize electroelastic coupling between the elastic displacement vector of components U_1, U_2, U_3 and the electric potential U_4 .

III. THE FORM OF SOLUTION

The piezoelectric wave is the solution of the elastic and electric equations that satisfy elastic and electric boundary conditions. When these waves attenuate exponentially inside the piezoelectric material, they are known as surface waves and if this is not the case they are known as bulk waves.

Consider the following form of the surface wave (partial wave)

$$U_i = u_i \exp(j\beta\alpha_i Y) \exp - j(\omega t - \beta(1 + j\gamma)X) \quad (11)$$

where $u_i(i=1, 2, 3)$ are the displacement amplitudes, $u_4(i=4)$ is the amplitude of the electric potential, k is the constant of propagation, the α_i are the penetration coefficients of the wave inside the piezoelectric substrate, γ is the coefficient of longitudinal attenuation and ω is the angular pulsation.

We will be interested in the coefficient α_i . With a chosen YX-cut LiNbO3 (Lithium Niobate).

Equations (9) and (10) can be written in a matrix form as

$$[A][U] = [0] \quad (12)$$

where $[A]$ is a matrix (4x4), the elements of this matrix depend on the features of the piezoelectric material (C_{ijkl} , ε_{ik} and e_{ij}) as well as of penetration coefficient α and of the acoustic velocity V_s .

The determinant of the matrix $[A]$ must be zero to ensure a non-trivial solution, it can be written as

$$\sum_{i=0}^8 \beta_i \alpha^i = 0 \quad (13)$$

where B_i depends on the features of the piezoelectric material (C_{ijkl} , ε_{ik} and e_{lij}) and of the acoustic velocity V_s .

The determinant of the matrix $[A]$ must be zero, we have eight complex roots ($i=1, \dots, 8$):

$$\alpha_i = a_i + jb_i \quad (14)$$

where a_i is the real part and b_i is the imaginary part, with $a_m = a_{m+1}$ and $b_m = b_{m+1}$ where $m=1, 3, 5, 7$.

In the surface mode (or Rayleigh wave) the α_i ($i=1, \dots, 4$) are conjugated by pairs and only the complex roots with negative imaginary part are taken into consideration (for convergence reasons).

Let us first neglect the longitudinal attenuation ($\gamma = 0$) and insert (14) in (11) to obtain

$$U_i = u_i \exp - (b_i k \cdot Y) \exp - j[\omega t - k(X + a_i Y)] \quad (15)$$

If we go inside the crystal (Y tends to $-\infty$), the wave U_i tends to zero. This corresponds to surface acoustic waves (SAW). In the opposite case (Y tends to $+\infty$), U_i tends to infinity ($+\infty$) (without physical signification).

Remarks

- ✓ If $\alpha_{re}^{(i)} = 0$ and $\alpha_{im}^{(i)} > 0$, ultrasonic pulse will be obtained and for a good detection of ultrasonic pulse we should have (Real part equals zero and the maximum positive value of Imaginary part (table 1)

IV. SUPPORT VECTOR MACHINE (SVM)

Support Vector Machine (SVM) is one the relatively modern methods that has showed high efficiently in recent years compared to older methods for classification including perceptron nervous systems. Work basis of SVM classification is data linearly classification and in linear division, we try to select a line that has more reliable edge (Figure 3).

To solve this equation, we should find optimum line for data by quadratic programming QP methods that are determined methods to solve limited problems. Before line division, we take data to higher dimensions via phi function to classify data with higher complexity in machine. We apply Lagrange Duality Theorem to transform minimization problem to duality form where we use simple function called core function that is vector coefficient of Phi function to solve a problem with very high dimensions. We can use different

core functions including exponential cores, vector and Sigmund [10-11].

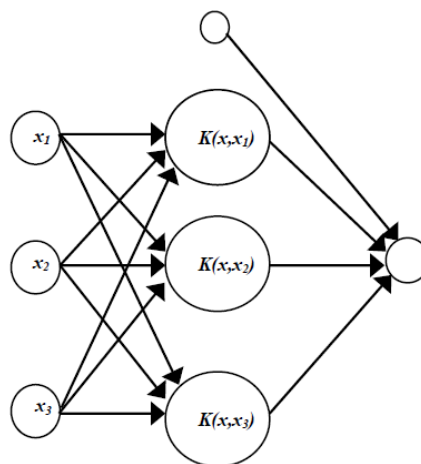


Figure 3. Architecture of SVM.

V. RESULTS AND DISCUSSION

Figure 4 shows the classification using SVM ; for each value of coefficient attenuation α_1 , we observe that Ultrasonic Pulse has 5 values , Figure 5 shows the classification using SVM but in this case the the classification factor is acoustic velocity V_s and this stag helps to know acoustic velocity V_s which corresponds to each value of coefficient attenuation α_1 , But in the attenuation α_2 we note that ; Ultrasonic Pulse is not detected , (Figure 6) , in this case we are not required to use the classification of acoustic velocity V_s , In the attenuation α_3 we note that ; Ultrasonic Pulse is not detected (Figure 7) (Table 1), in this case we are not required to use the classification of acoustic velocity V_s . Figure 8 shows the classification using SVM ; for each value of coefficient attenuation α_4 , we observe that Ultrasonic Pulse has 4 values , Figure 9 shows classification for acoustic velocity corresponds to each value of coefficient attenuation α_4 .(Table 1)

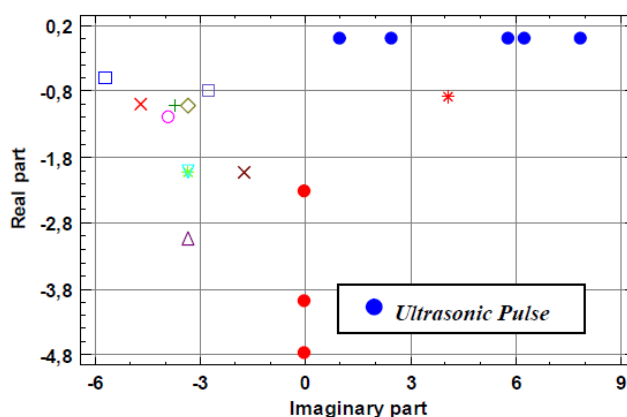


Figure 4: SVM classifier for α_1 .

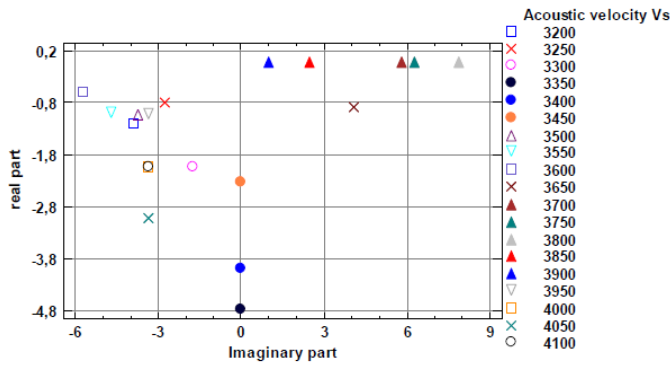


Figure 5. SVM classifier for $\alpha 1$ - Classification factor Vs

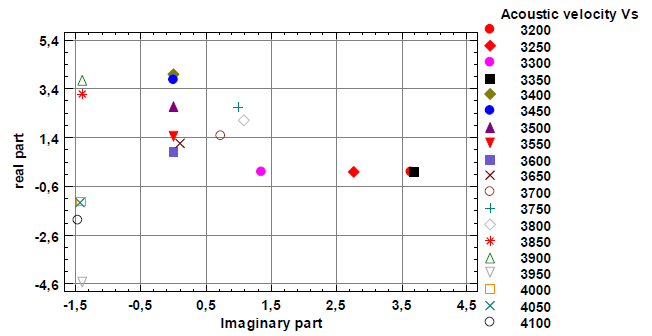


Figure 9: SVM classifier for $\alpha 4$ - Classification factor Vs

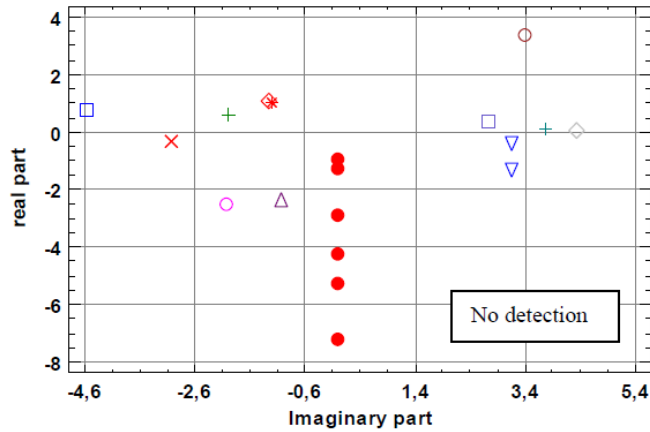


Figure 6. SVM classifier for $\alpha 2$.

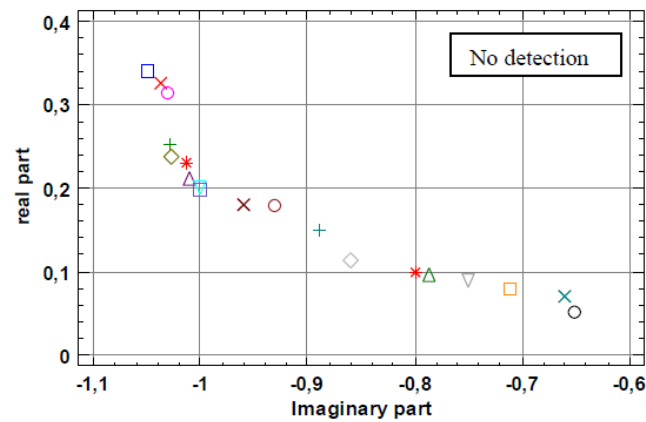


Figure 7: SVM classifier for $\alpha 3$.

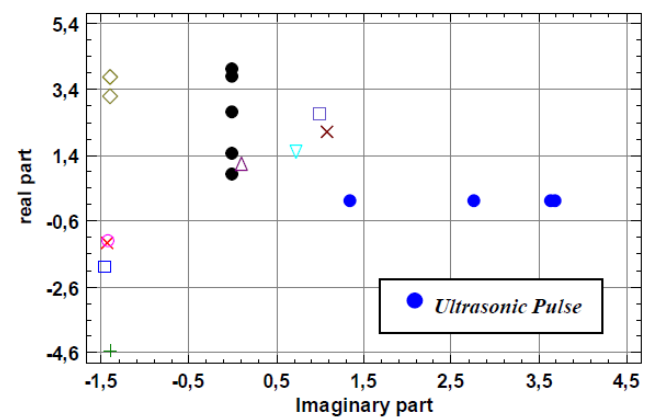


Figure 8: SVM classifier for $\alpha 4$.

TABLE I. SUMMARIZES THE FULL WORK

Coefficient attenuation	Real part	Imaginary part	Acoustic velocity Vs (m/s)	Ultrasonic Pulse
$\alpha 1$	0	5,78765	3700	Detection
	0	6,25443	3750	Detection
	0	7,8765	3800	Good Detection
	0	2,4543	3850	Detection
	0	1,00001	3900	Detection
$\alpha 2$	No values	No values	No values	No detection
$\alpha 3$	No values	No values	No values	No detection
$\alpha 4$	0	3,65	3200	Detection
	0	2,765	3250	Detection
	0	1,34571	3300	Detection
	0	3,7	3350	Good Detection

VI. CONCLUSION

In this article, we explained that the phenomenon of Ultrasonic Pulse or acoustics bulk microwaves are relying on numerical results at the level of attenuation coefficients. Changes in real and imaginary parts of the coefficients based on the acoustic velocity to detect these waves. It is quite clear that these waves are propagant into the piezoelectric material considered. Our method is applicable for any piezoelectric material, you just have to change the characteristics of the material parameters. The positive feature of this work gives us accurate values.

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satellite.